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Deep learning for healthcare applications based on physiological signals: a review

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Abstract

Background and Objective: We have cast the net into the ocean of knowledge to retrieve the latest scientific research on deep learning methods for physiological signals. We found 53 research papers on this topic, published from 01.01.2008 to 31.12.2017.

Methods: An initial bibliometric analysis shows that the reviewed papers focused on Electromyogram (EMG), Electroencephalogram (EEG), Electrocardiogram (ECG), and Electrooculogram (EOG). These four categories were used to structure the subsequent content review.

Results: During the content review, we understood that deep learning performs better for big and varied datasets than classic analysis and machine classification methods. Deep learning algorithms try to develop the model by using all the available input.

Conclusions: This review paper depicts the application of various deep learning algorithms used till recently, but in future it will be used for more healthcare areas to improve the quality of diagnosis.

Keywords: Deep learning, Physiological signals, Electrocardiogram, Electroencephalogram, Electromyogram, Electrooculogram

1. Introduction

Physiological signals are an invaluable data source which assists in disease detection, rehabilitation, and treatment [1]. The signals come from sensors implanted or placed on the skin [2]. The application areas dictate where the sensors are to be placed [3, 4]. In turn, the sensor location determines the characteristics of the physiological signal. Relevant information must be extracted from the physiological signal in order to support a specific healthcare application [5, 6]. It is difficult to establish what constitutes relevant information, because various medical ontologies can be used for data interpretation [7]. It is unavoidable that these ontologies contain conflicts and inconsistencies [8]. Another fundamental problem is that physiological signal interpretation suffers from intra-individual variability [9]. For example, both electrode position and noise influence the signal waveform [10]. Therefore, human interpretation requires years of training to acquire specialized knowledge. Even with expert knowledge, manual physiological signal interpretation suffers from intra- and inter-operator variability [11]. Furthermore, physiological signal interpretation is a tiresome process where human errors can be caused by fatigue [12, 13]. Computer supported signal analysis is not affected by fatigue related mistakes and it can also eliminate both intra- as well as inter-observer variability. In addition, most computer based analysis interpretation can be done quicker and more cost effective when compared to

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human interpretation [14]. Having established the need for computer based physiological signal analysis, we have to find the most appropriate processing methods for a given healthcare application.

Nowadays, performance measures, such as classification accuracies [15, 16], govern computer based analysis and classification of physiological signals for healthcare applications [17, 18, 19]. The goal is to design algorithms that outperform the established methods [20]. The design process is based on the idea of having an offline and online system, as shown in Figure 1 [21, 22]. The offline system is used to design the required algorithm structure based on labeled data. That algorithm structure is used in the online system to process measurement data. In most of the cases, the system consists of three sequential processing steps: 1) preprocessing [23, 24], 2) feature extraction [25, 26] 3) classification [27]. The first two steps establish the analysis system which extracts information from the physiological signal. This approach is very target directed, since the design process is governed by the feature performance. However, real competition is difficult to establish, because the underlying testing data are rarely comparable. Another problem is that, there is no way of knowing which feature extraction algorithm is suitable for a given problem. The feature quality can only be established a posteriori with statistical methods [28, 29]. This situation is dis-satisfactory for *two* reasons. Various feature extraction algorithms must be evaluated on the physiological signals before selecting the best performing feature extraction method. Even the increased effort fails to ensure that the most relevant information are extracted. The second reason comes from the fact that only a small number of features are used for decision making, because the performance of decision making algorithms deteriorates for higher dimensional inputs [30]. Hence, the main design goal of current decision support systems is to restrict the amount of information that underpins the decision making [31]. Having to restrict the amount of information for the decision-making process is a big problem, because the decision quality will suffer. The negative effects become more prominent for large and diverse physiological signal datasets that hold the information to tackle more challenging application areas, such as Brain Computer Interface (BCI), cardiovascular diseases, sleep apnea, sleep stages and muscular abnormalities.

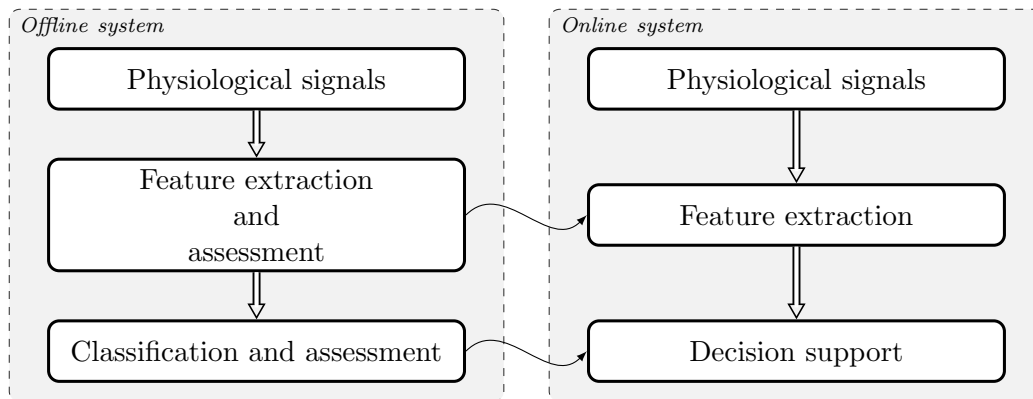


Figure 1: Block diagram for the design of a traditional decision support system based on physiological signals.

Current decision-making systems under-perform for large and varied datasets, because they fail to process information that is sufficiently diverse to cover all scenarios. More depth is required to represent all the information in a dataset. Fundamentally, we require implicit knowledge to make good decisions based on the information extracted from physiological signals. In the past, that implicit knowledge was exclusively found in highly skilled medical practitioners. Deep learning was designed to overcome these shortcomings by taking into consideration all information a training dataset has to offer. The method promises to establish implicit knowledge in a machine. In this review, we investigate the validity of this claim by analysing the ways in

which deep learning has been applied to physiological signals. We found promising research in the areas of Electrocardiogram (ECG), Electroencephalogram (EEG), Electromyogram (EMG) and Electrooculogram (EOG) based healthcare applications. However, the amount of research work does not reflect the diversity of healthcare application that can benefit from physiological signal interpretation. Therefore, we adopt the position that the diversification of the research is needed. The depth and specialization must come from training the deep learning algorithms with larger and more varied data sets.

To support our claim that deep learning is a major step towards understanding physiological signals, we have organized the remainder of the paper as follows. The next section establishes the importance of implicit knowledge for physiological signal interpretation and it provides background on deep learning. Section 3 presents bibliometric and content analysis results. Based on these results, we put forward a range of research gaps in the discussion section. In this section, we have also discussed limitations and future work. The paper concludes with Section 5.

2. Background

Physiological signals reflect the electrical activity of a specific body part [6]. As such, the electrical activity provides information about the physiological condition. Traditionally, this information can be used by medical practitioners for decision making [32, 33]. These decisions have far reaching consequences on diagnosis, treatment monitoring, drug efficacy tests, and quality of life. From a machine learning perspective, a medical practitioner is an intelligent agent who makes good decisions. In order to reach these decisions some sort of knowledge is required. This knowledge shapes the process which generates actions from both state and input. For example, a clinician analyses an ECG signal. As that analysis process continues, there is a growing suspicion that the signal was taken from a patient with coronary artery disease. More and more suspicious waveform segments emerge until a positive diagnosis is reached. From a processing perspective, the ECG signal is the input, the reading clinician is the system and the system state is reflected in the growing suspicion.

In its simplest form, knowledge can be explicitly expressed as mathematical rules and physical facts. Engineers make use of this explicit knowledge to create expert systems [34]. However, these systems are limited to a specific domain and they operate in highly controlled environments. Only for these environments, we are reasonably sure about the physical facts and mathematical rules which shape the correct behaviour. Furthermore, expert systems don't reflect the concept of suspicion and common sense. Overcoming these limitations requires implicit knowledge which can be found in the complex wiring and the synaptic setup of biological brains as well as the mechanical and sensory properties of biological bodies. The only way for computers to mimic implicit knowledge is to learn from examples. The idea is to find a way to learn general features in order to make sense of new data. This description highlights the central role of data for establishing implicit knowledge. The amount of data must be sufficiently large to provide many training examples from which a large set of parameters can be extracted. Only a large number of parameters give rise to the richness of class functions which model the implicit knowledge.

Deep learning is a change in basic assumptions of artificial intelligence algorithm design [35]. This change percolates through to all application areas of machine learning, such as computer vision, speech recognition, natural language processing and indeed diagnosis support [36]. Central to deep learning are the ideas of parallel processing and networked entities. The next section details these ideas by discussing the deep learning methods.

2.1. Deep Learning Methods

Deep learning belongs to the class of machine learning methods. It is a special form of representation-based learning, where a network learns and constructs inherent features from

each successive hidden layer of neurons [31]. The term “deep” is derived from the numerous hidden layers in the Artificial Neural Network (ANN) structure.

The ANN algorithm models the functionality of a biological brain [37]. The model is realized with a structure that is made up of input-, hidden-, and output-layers, as shown in Figure 2. Every neuron or node (nerve cell) is connected to each neuron in the next layer through a connection link. A nerve cell is made up of axon (output), dendrites (input), a node (soma), nucleus (activation function), and synapses (weights) [38]. The activation function in the artificial neuron acts as the nucleus in a biological neuron whereas the input signals and its respective weights model the dendrites and synapses respectively. Figure 3 illustrates the neuron structure.

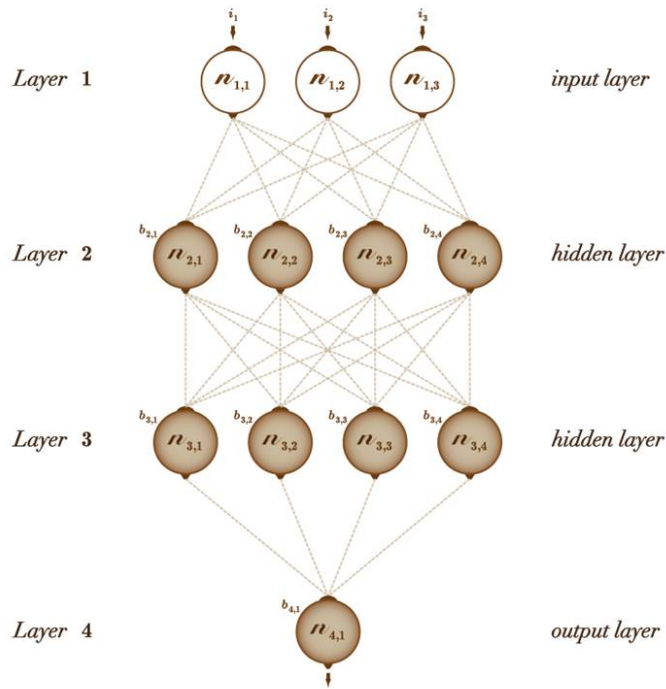


Figure 2: Traditional ANN

Unfortunately, the ANN structure is receptive to translation and shift deviation, which may adversely affect the classification performance [39]. To eliminate these shortcomings, an extended version of ANN, the Convolutional Neural Network (CNN), was developed [40]. The CNN architecture ensures translation and shift invariance [41]. Figure 4 illustrates a generic CNN network structure. It is a feed-forward network, which comprises of: convolution, pooling, and fully-connected, layers [41]. They are briefly explained below.

1. Convolution layer: The input sample is convolved with a kernel (weights) in this layer. The output of this layer is the feature map. The stride controls how much the kernel convolves with the input sample. The convolution operation acts as a feature extractor by learning from the diverse input signals. The extracted features can be used for classification in subsequent layers. Figure 5 illustrates a convolution operation between f (input) and g (kernel), giving an output c . Equations 1 and 2 provide an example of the convolution

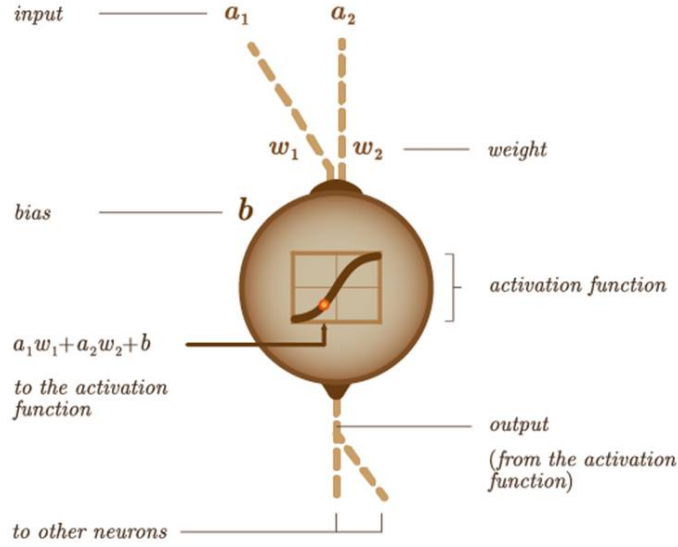


Figure 3: Neuron structure

calculation.

$$\begin{aligned}
 c(1) &= 1 \times 3 + 2 \times 4 + 3 \times 1 = 14 \\
 c(2) &= 2 \times 3 + 3 \times 4 + 4 \times 1 = 22 \\
 c(3) &= 3 \times 3 + 4 \times 4 + 5 \times 1 = 30
 \end{aligned} \tag{1}$$

$$\begin{aligned}
 \text{Output1} &= 22 \times W_1 + 38 \times W_3 + 54 \times W_5 \\
 \text{Output2} &= 22 \times W_2 + 38 \times W_4 + 54 \times W_6
 \end{aligned} \tag{2}$$

2. Pooling layer: This is a down-sampling layer where the pooling operation is employed to reduce the spatial dimension of the input sample, while retaining the significant information. The pooling operation can be average, max, or sum. The max-pooling operation is typically employed. An example of a max-pooling operation, with a stride of 2, is shown Figure 6. In this example, the number of input samples are halved by retaining only the maximum value within a selected stride. In a stride that contains 14 and 22, the value 22 is retained, and, 14 is discarded.
3. Fully-connected layer: Fully-connected signifies that each neuron in the previous layer is connected to all the neurons in the current layer. The total number of fully-connected neurons in the final layer determines the number of classes. Figure 7 provides a graphical representation of a fully-connected layer. The neurons are all connected and each connection has a specific weight. This layer establishes a weighted sum of all the outputs from the previous layer to determine a specific target output.

A leaky rectifier linear unit [42] is used as an activation function after the convolution layer. The purpose is to map the output to the input set and introduce non-linearity as well as sparsity to the network. The CNN is trained with backpropagation [43] and the hyperparameters may be tuned for optimal training performance.

In addition to CNN, there are other deep learning architectures, such as autoencoder [44], deep generative models [45] [46] and Recurrent Neural Network (RNN), that can be used to monitor the physiological signals [47].

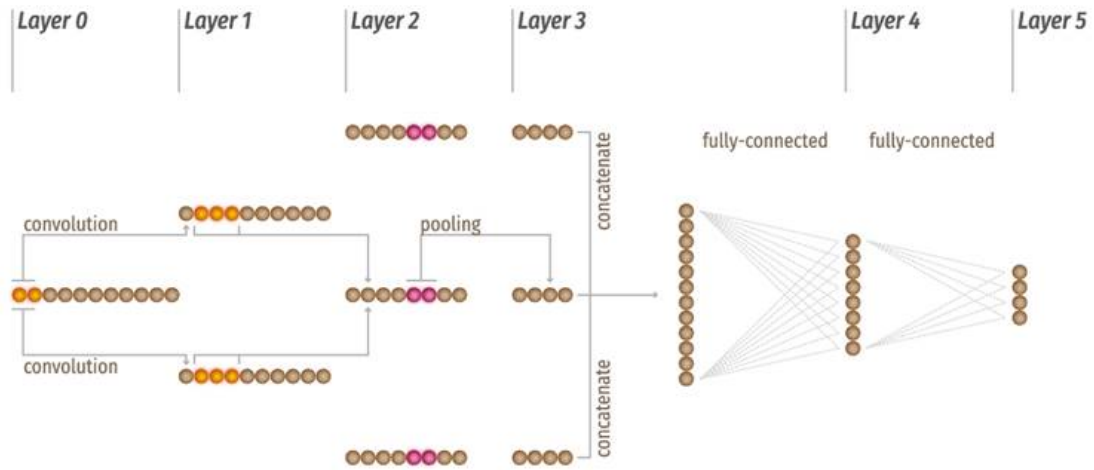


Figure 4: CNN network structure

$$c = f * g$$

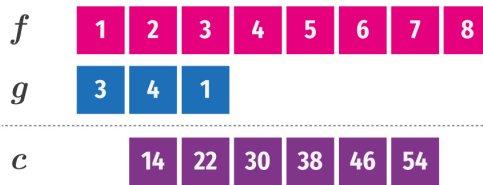


Figure 5: Convolution layer

The autoencoder is an unsupervised neural network that is trained to imitate the input to its output. The dimension of the input is the same as the dimension of the output. The encoders are stacked together to form a deep autoencoder network. The autoencoder takes unlabelled inputs, encodes these inputs, and subsequently it reconstructs the inputs as precisely as possible. Hence, the network structure must determine which data features are significant. An autoencoder consists of *three* layers: input, output, and hidden. Encoding and decoding are the two main steps in the autoencoder algorithm. During encoding and decoding, the same weights are employed to encode the feature and reconstruct an output sample in the output. Autoencoders are trained with a backpropagation algorithm that employs a metric known as the loss function [43]. That function computes the amount of information which is lost during input reconstruction. Thus, a network structure with a small loss value will produce a reconstruction that is nearly identical to the input sample [37].

Deep Belief Network (DBN) [45] and Restricted Boltzmann Machine (RBM) [48] are common forms of the deep generative model, where DBNs are stacked layers of RBM. The RBM is made up of a two-layer neural net with one visible and one hidden layer. Each node in the layer learns a single feature from the input data by making random decisions on whether to transmit the input or not. The nodes in the first (visible) layer are connected to every node in the second (hidden) layer. The RBM takes the inputs and translates them into a set of numbers that encode

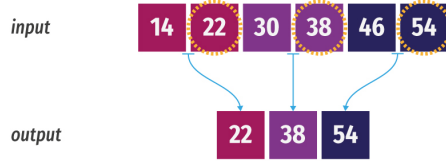


Figure 6: Max pooling layer

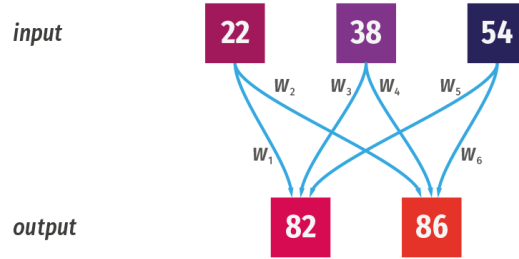


Figure 7: Fully connected layer

the inputs. Then, a backward translation is implemented to reconstruct the inputs. The RBM network is trained to reconstruct through forward and backward passes [49, Chapter 6].

The DBN is a probabilistic model with several hidden layers [50]. It can be efficiently trained by using a technique known as greedy layer-wise pre-training [51]. Typically, the DBNs are stacked layers of RBM. The first layer of the RBM is trained to reconstruct its input. After which, the first hidden layer is considered as the visible layer and it is trained using the outputs from the input layer. This process is iterated until all layers in the structure are trained [45].

In contrast to the feed-forward network, the RNN employs a recursive approach (recurrent network) whereby the network performs a routine task with the output being dependent on the previous computation. This functionality is created with inbuilt memory. The most common type of RNN is the Long Short-Term Memory (LSTM) network [52]. It has the capability to learn long-term dependencies. The LSTM algorithm incorporates a memory block with three gates: the input, output, and forget gate. These gates control the cell state and decide which information to add or remove from the network. This process repeats for every input.

1. Input gate: decides what new information is to be stored and updated in the cell state.
2. Output gate: judges what information is used based on the cell state.
3. Forget gate: evaluates what information is redundant and discards it from the cell state.

These deep learning architectures have demonstrated their potential by surpassing the performance of traditional machine learning techniques [31]. Furthermore, deep learning algorithms minimize the need for feature engineering. The next section, focuses on scientific work that applied deep learning to physiological signal interpretation for health care applications.

3. Review

In this review, we consider 53 articles focusing on deep learning methods applied to physiological signals for healthcare applications. These papers were published in the period from 01.01.2008 to 31.12.2017. Figure 8 shows the yearly distribution of 53 articles together with a trend line [53]. Apart from the data distribution, the figure also features a trend line which was

generated with a linear regression approach [54]. The large positive gradient of the trend line indicates more papers, on this topic, published in recent years.

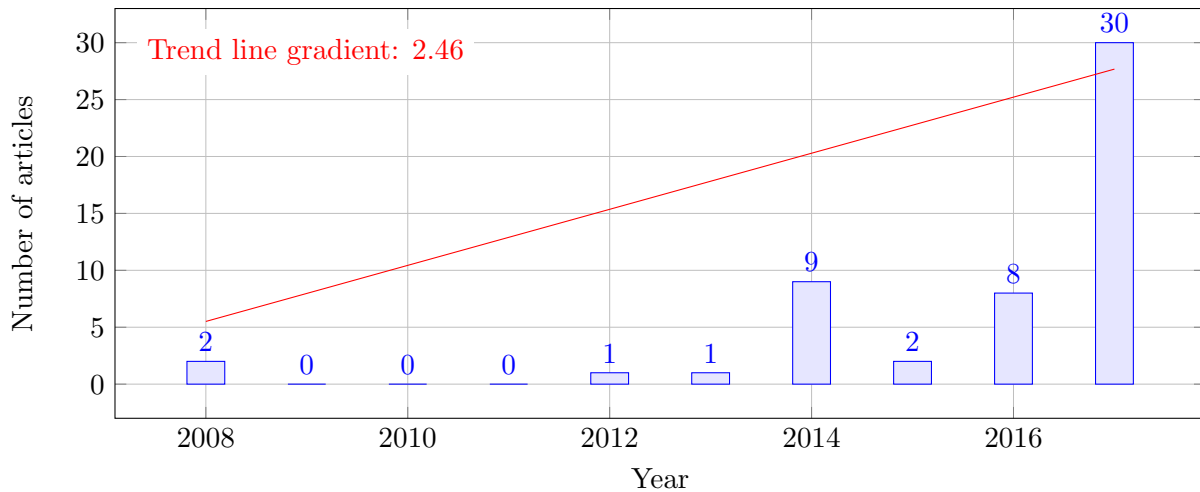


Figure 8: Number of articles on deep learning, published each year from 01.01.2008 to 31.12.2017

Our review of the 53 articles is based on *two* analysis methods. The first method is a bibliometric analysis, which helps us to detect the structure that governs relationship between the paper topics. We use this information to arrange the second analysis method, which deals with the content of the reviewed papers. The paper content is dissected in terms of common parameters that enable us to compare the studies across different healthcare applications.

3.1. Bibliometric analysis

The bibliometric analysis establishes the topic structure of the reviewed papers. This unlocks the paper content. We have used the well-known VOSviewer¹ software to establish a co-occurrence network [55, 56]. Before feeding the data to the VOSviewer algorithm, we created a thesaurus file to group keywords, having the same meaning, into broader topics. Table A.8 shows that mapping. Figure 9 shows the co-occurrence network and the topic clusters. Table 1 reveals the topic structure by aligning the topics to clusters. These clusters are centred on a specific physiological signal. To be specific, the largest topic cluster² includes EMG. The physiological signals are widely used in healthcare areas, such as speech, prosthesis and rehabilitation robotics. CNN is the deep learning method of choice in this cluster. The second cluster is related to the EEG which is used for BCI. the cluster shows that noise is a problem for EEG processing. Cluster 3 focuses on ECG, which is linked to Cardiovascular Disease (CVD), arrhythmia and Automated External Defibrillator (AED). The last cluster deals with EOG which can be used to detect sleep problems. The deep learning methods of DBN and RNN are used to the detect of Obstructive Sleep Apnea (OSA) using different physiological signals. The clustering helps us to structure the content review, which is presented in the next section.

3.2. Content review

The bibliometric research shows *four* distinct clusters focused on four physiological signals namely: ECG, EEG, EMG and EOG. They are briefly discussed in the following sections.

¹Web page (Last accessed 11.12.2017): <http://www.vosviewer.com/>

²In terms of the number of papers that include a keyword that was mapped to the cluster topics.

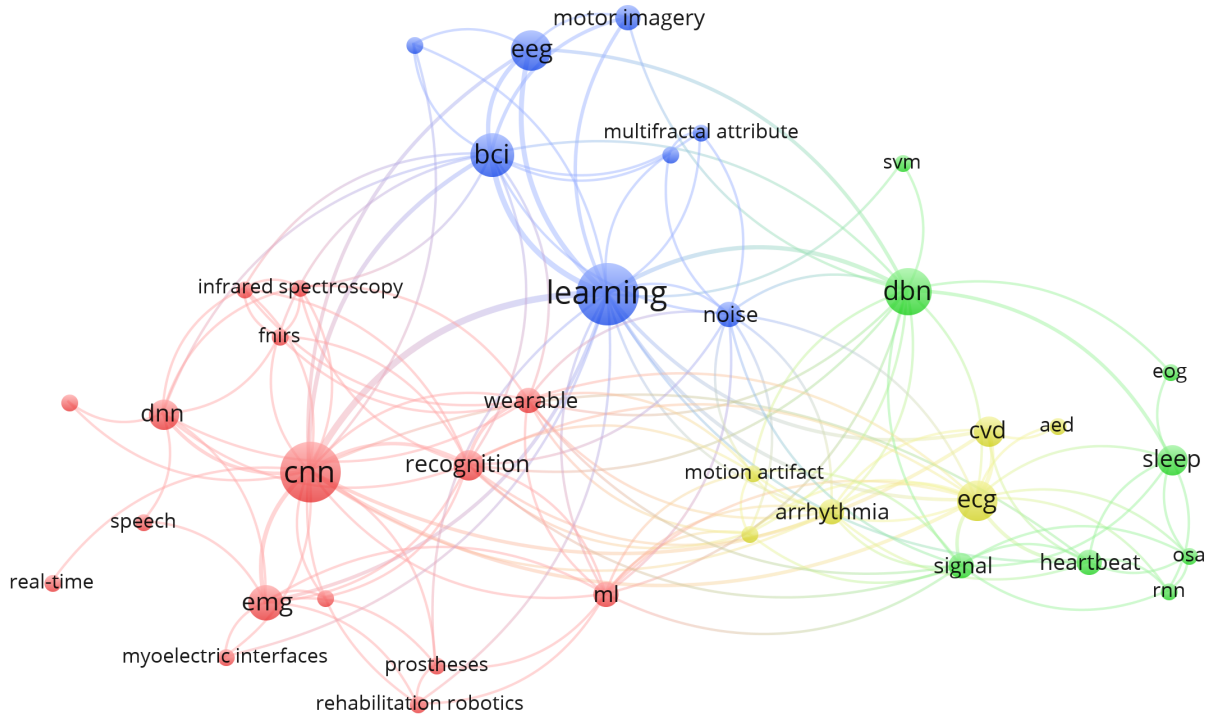


Figure 9: Network visualization for the author supplied keywords

Table 1: Topic cluster summary, where C is the Cluster number. Colour indicates the cluster colour as shown in Figure 9.

| C | Topics | Colour |
|---|-----------------------------------------------------------------------------------------------------------------------------------------------------------------------------------------------------------------|--------|
| 1 | emg , cnn, cognitive states, dnn, fnirs, hand gesture, infrared spectroscopy, ml, myoelectric interfaces, prostheses, real-time, recognition, rehabilitation robotics, speech, wearable, word generation | Red |
| 2 | eeg , bci, learning, motor imagery, multifractal attribute, neuromorphic computing, noise, wavelet leader | Blue |
| 3 | ecg , aed, arrhythmia, contaminant mitigation, cvd, motion artifact | Yellow |
| 4 | eog , dbn, heartbeat, osa, rnn, signal, sleep, svm | Green |

Table 2: Summary of works carried out using DL algorithms with EMG signals.

| Author | Application | DL algo- rithm | Data | Results |
|---------------------------------|------------------------------|---------------------------|-----------------------------------------------------------|------------------------------------------------------------------|
| Xia et al., 2017 [60] | Limb movement estimation | RNN | Measurements from eight healthy subjects | The RNN outperforms other methods for estimating a 3D trajectory |
| Zhai et al., 2017 [61] | Neuroprosthesis control | CNN | NinaPro Database (DB)2&3 [62] | accuracy: 83% |
| Park et al., 2016 [63] | Movement intention decoding | CNN | Kinematic and EMG data NinaPro DB [64] | accuracy: > 90% |
| Atzori et al., 2016 [65] | Hand movement classification | CNN | NinaPro DB [62] | accuracy: 66.59% |
| Geng et al., 2016 [66] | Gesture recognition | CNN | 18 subjects performing 16 gestures each recorded 10 times | accuracy: 99.5% |
| Wand and Schmidhuber, 2016 [67] | Speech recognition | Deep Neural Network (DNN) | EMG-UKA Corpus [68] | DNN outperforms a Gaussian Mixture Model (GMM) front end |
| Allard et al., 2016 [69] | Robotic arm guidance | CNN | 18 subjects performing 7 gestures | accuracy: \approx 97.9% |
| Wand and Schultz, 2014 [70] | Speech recognition | DNN | 25 sessions from 25 subjects | Visualization of hidden nodes activity |

3.2.1. Deep learning methods applied to EMG

The EMG measures the electrical activity of skeletal muscles [57]. The electrical sensors, known as electrodes, are placed on the skin above the muscles of interest [58]. The EMG signals indicate: muscle activation, force produced by the muscle, and muscle state [59]. All these factors are superimposed, i.e. the EMG signal measurement picks up the contributions from different sources and sums them up. Hence, it is difficult to gain information about one particular aspect by observing the EMG signal. Table 2 details the research work which describe the deep learning methods used to analyze the EMG signal. Individual columns healthcare application area, Deep Learning (DL) algorithm, the data used for the study, and the study results. As such, the DL algorithms were introduced in Section 2.1.

3.2.2. Deep learning methods applied to EEG

The EEG is measured by placing electrodes on the skull of the subject, where they pick up the electrical activity of the brain [71, 72]. As such, that activity results from firing neurons emitting action potentials. At any given time, the electrode sums up many charges from different sources. The resulting EEG signal has a noise like characteristic, which makes the interpretation difficult. Furthermore, the signal is affected by EOG and EMG artifacts [73, 74, 75]. It takes the trained eye of a practitioner to spot the features that indicate a specific mental state [76]. One of the main drivers behind the application of DL algorithms applied to EEG is BCI [77]. The real-time nature of this application makes human signal interpretation impossible [78]. Hence, BCI requires automated decision making. Table 3 lists the reviewed research works conducted using deep learning with EEG signals. The list contains one exception, Huve et al. used functional near-infrared spectroscopy [79] to track neural dynamics of the brain [80].

3.2.3. Deep learning methods applied to ECG

The ECG is measured by placing electrodes on the chest [81]. These electrodes record the electrical activity of the human heart [82]. The signal reflects the functioning of the heart and it has well distinguishable features, even in the time domain. The difficulty in ECG interpretation is to spot the morphological changes which indicate a particular cardiac problem [83, 84] or diabetes [85, 86]. These abnormalities may be minute and very often they may be transients or present all the time [87]. The research work, listed in Table 4, discusses the DL algorithms used for the automated detection of various cardiac abnormalities. The scientific work, described in 13 out of 14 reviewed papers, relies on measurements which were taken from public DBs. Therefore, the results can be compared with state-of-the-art methods. For example, Acharya et al. [88] reported the performance measures obtained through the deep learning system alongside the performance figures of the traditional diagnosis support systems. Their system outperformed traditional approaches and it has the added benefit of not having to perform feature extraction and de-noising. Table 4 lists the works reported on deep learning applied to ECG signals.

3.2.4. Deep learning methods applied to EOG and a combination of signals

The EOG measures the corneo-retinal standing potential which occurs between back and front of the human eye. Two electrodes are placed either left and right of the eye or above and below the eye. The signal can be used to detect eye movements [89]. It is useful for ophthalmological diagnosis [90]. However, the EOG is affected by noise and artifacts, that makes the signal interpretation difficult [91]. Table 5 details research work which aims to overcome these difficulties with deep learning algorithms. Only Zhu et al. applied the deep learning algorithm exclusively to EOG signals. Table 5 presents a summary of works carried out using DL algorithms with EOG and other physiological signals.

Table 3: Summary of works carried out using DL algorithms with EEG signals.

| Author | Application | DL algo- rithm | Data | Results |
|------------------------------------|--------------------------------------------------------------------------------------|-------------------|------------------------------------------------------------------------------------------------------------|------------------------------------------------------------------------------------------|
| Fraiwan et al., 2017 [93] | Sleep state identifica- tion | Autoencoders | Measurements [94] | 80.4% accuracy |
| Schirrmeister et al., 2017 [95] | EEG decoding and visu- alization | CNN | BCI competition IV dataset 2a [96] and measurement data | Up 89.8% accuracy |
| Hosseini et al., 2017 [97] | Epileptogenicity local- ization | CNN | EEG and rs-fMRI measure- ments from the ECoG dataset [98] | Normal p-value 1.85e-14, p- Seizure value 4.64e-27 |
| Schirrmeister et al., 2017 [99] | Decoding excited move- ments | CNN | Not reported | Accuracy comparable to stan- dard methods |
| van Putten et al., 2017 [100] | Butcome prediction for patients with a postanoxic coma after cardiac arrest | CNN | EEGs from 287 patients at 12 h after cardiac arrest and 399 patients at 24 h after cardiac arrest | Sensitivity of 58% at a speci- ficity of 100% for the predic- tion of poor outcome |
| Spampinato et al., 2017 [101] | Discriminate brain ac- tivity | CNN | Six subject were shown 2000 images in 4 sessions | Accuracy 86.9% |
| Kiral-Kornek et al., 2017 [102] | BCI | CNN | 6 subjects up to 1000 individ- ual hand squeezes | Power comparisons of various processing platforms. |
| Acharya et al., 2017 [103] | Seizure detection | CNN | Freiburg EEG DB [104, 105, 106, 107, 108] | accuracy: 88.67% |
| Lu et al., 2017 [109] | Motor imagery classifi- cation | RBM | BCI competition IV data set 2b [110, 111, 112] | Accuracy has been improved about 5% compared with other methods. |
| Huve et al., 2017 [80] | Tracking of neural dy- namics | CNN, DNN | 1 subject 180 trials | DNN outperforms CNN |
| Hajinoroozi et al., 2016 [113] | Prediction of driver's cognitive performance | CNN | 37 subjects, 70 sessions | Area under the receiver oper- ating characteristic: 86.08 |
| Nurse et al., 2016 [114] | BCI | CNN | 1 subject 30 min of data | accuracy 81% |

| | | | | |
|-------------------------------------|----------------------------------------------|-----------------------|---------------------------------------------------------------------------------------------------------|------------------------------------------------------------------------------------------|
| Jingwei et al., 2015 [115] | Response representation | CNN | EEG motor activity data set [116] | accuracy: 100% |
| Hajinoroozi et al., 2015 [117] | Prediction of driver's cognitive performance | CNN | 37 subjects, 80 sessions | Area under the receiver operating characteristic: 82.78 |
| Jirayucharoensak et al., 2014 [118] | Based Emotion Recognition | Deep learning network | DEAP Dataset [119] | valence accuracy: 49.52%, arousal accuracy 46.03% |
| An et al., 2014 [120] | Based Emotion Recognition | Deep learning network | 4 subjects 60 trials | valence accuracy: 49.52%, arousal accuracy 46.03% |
| Zheng et al., 2014 [121] | Emotion classification | DBN | 6 subjects 2 trials each | accuracy: 87.62% |
| Li and Cichocki, 2014 [122] | Motor imagery | DBN | 3 subjects performing motor imagery tasks in four sessions. Each session had 15 trails. | Accuracy: 96% |
| Jia et al., 2014 [123] | Affective state recognition | RBM | DEAP Dataset [119] | RBM-based model to extract representative features and to reduce the data dimensionality |
| Ren and Wu, 2014 [124] | Feature extraction | CNN | Dataset III in 2003 BCIC II, Dataset Iva in 2005 BCIC III, Dataset III in 2005 BCIC III [110, 111, 112] | Accuracy: 87.33% |
| Ahmed et al., 2013 [125] | Detecting target images | DBN | Not specified | DBN outperforms SVM. |
| Mirowski et al., 2008 [126] | Epileptic seizure prediction | CNN | Freiburg EEG DB [104, 105, 106, 107, 108] | zero-false-alarm seizure prediction on 20 patients out of 21 |
| Cecotti and Graeser, 2008 [127] | Motor imagery classification | CNN | 2 subjects 5 trails of about 3 minutes | Recognition accuracy: 53.47% |

Table 4: Summary of works carried out using DL algorithms with ECG signals.

| Author | Application | DL algo- rithm | Data | Results |
|--------------------------------|----------------------------------------------------------------------------|---------------------------------|----------------------------------------------------------------------------------------------------------------|------------------------------------------------------------------------------------------------|
| Acharya et al., 2017 [128] | Arrhythmia detection using different intervals of tachycardia ECG segments | CNN | MIT-BIH arrhythmia database [129] | Accuracy of 92.50%, sensitivity of 98.09%, specificity of 93.13% |
| Tan et al., 2017 [130] | Coronary artery disease signal identification | LSTM, CNN | Physionet databases: Fantasia (for Normal) and St.-Petersburg Institute of Cardiology Technics (for CAD) [129] | Accuracy of 99.85%. |
| Acharya et al., 2017 [131] | Coronary artery disease detection | CNN | Physionet databases: Fantasia (for Normal) and St.-Petersburg Institute of Cardiology Technics (for CAD) [129] | Accuracy of 94.95% and 95.11% are obtained for two and five seconds ECG segments respectively. |
| Pourbabae et al., 2017 [132] | Features for Screening Paroxysmal Atrial Fibrillation | CNN | The PAF prediction challenge database [133] | Precision=93.6% |
| Zheng et al., 2017 [134] | ECG identification | DNN | MIT arrhythmia database [135] and self-collected data | 94.39% recognition rate |
| Majumdar et al., 2017 [136] | Arrhythmia classification | Robust deep dictionary learning | MIT arrhythmia database [135] | 97.0% recognition rate |
| Shashikumar et al., 2017 [137] | Monitoring and detecting atrial fibrillation | CNN | 98 subjects, 45 with atrial fibrillation and 53 with other rhythms. | Up to 91.8% accuracy |

| | | | | |
|-----------------------------|-------------------------------------------|-------------------------------|-----------------------------------------------------------------------------------------------------------------------------------------------------------------------|------------------------------------------------------------------------------------------|
| Acharya et al., 2017 [88] | Detection of myocardial infarction | CNN | lead II from the ECG DB (Physikalisch-Technische Bundesanstalt diagnostic ECG DB) [129] | accuracy: 93.18% |
| Lou et al., 2017 [138] | Heartbeat classification | DNN | Lead II from the MIT-BIH arrhythmia DB [135] | Accuracy: 97.5% |
| Acharya et al., 2017 [139] | Identification of ventricular arrhythmias | CNN | MIT-BIH arrhythmia DB (MITDB) [129, 135], MIT-BIH malignant ventricular arrhythmia DB (VFDB) [140], Creighton University ventricular tachyarrhythmia DB (CUIDB) [141] | accuracy: 92.50% |
| Acharya et al., 2017 [142] | Heart beat classification | CNN | MIT-BIH arrhythmia DB [129] | accuracy: 94.03% |
| Cheng et al., 2017 [143] | Sleep apnea detection | RNN | ECG sleep apnea DB [144] | accuracy: $\approx 90\%$ |
| Taji et al., 2017 [145] | Signal quality classification | RBM | MIT-BIH arrhythmia DB [129] | accuracy: 99.5% |
| Lou et al., 2017 [138] | Heartbeat classification | RBM | MIT-BIH arrhythmia DB [135] | RBM-based model to extract representative features and to reduce the data dimensionality |
| Muduli et al., 2017 [146] | Fetal-ECG signal reconstruction | Stacked Denoising Autoencoder | Abdominal non-invasive FECG DB [129] | accuracy: 99.5% |
| Kiranyaz et al., 2016 [147] | Heart beat classification | CNN | MIT/BIH arrhythmia DB [129] | accuracy: 99% |
| Zheng et al., 2014 [148] | Congestive heart failure detection | CNN | BIDMC Congestive Heart Failure data set [129] | accuracy: 94.67% |

Table 5: Summary of works carried out using DL algorithms with EOG and other signals.

| Author | Application | Signal | DL algo- rithm | Data | Results |
|------------------------------|------------------------------------------|---------------|-------------------|--------------------------------------------------------------------------------------------------------------------------------------|-----------------------------------------------------------|
| Du et al., 2017 [149] | Driving fatigue detection | EOG and EEG | Autoencoder | Measurements from 21 subjects | Correlation Coefficient 0.85, Root Mean Square Error 0.09 |
| Zhang et al., 2017 [150] | Momentary mental workload classification | EOG, EEG, ECG | CNN | 6 subjects and 2 sessions each | Accuracy: 93.8% |
| Xia et al., 2017 [151] | Sleep stage classification | EOG, EEG | DBN | sleep EDF DB [Expanded] in Physionet [129, 152] | Accuracy: 83.3% |
| Zhu et al., 2014 [153] | Drowsiness detection | EOG | CNN | 22 subjects and 22 sessions each | mean correlation coefficient of 0.73 |
| Långkvist et al., 2012 [154] | Sleep Stage Classification | EOG, EEG, EMG | DBN | 25 acquisitions from PhysioNet [129] for training and testing and Home Sleep Dataset 60 hours from normal one subject for validation | 72.2% |

4. Discussion

Even though the deep learning is still in its infancy, published studies have shown that it possesses the capability of faster and more reliable diagnoses in physiological signals. That potency may well trigger a shift away from the currently used decision support methods, such as Support Vector Machine (SVM) and K-Nearest Neighbour (K-NN), towards deep learning [92]. It can be noted from Table 4 that the employment of deep learning in ECG signals yielded promising diagnostic performances. This is because the developed model is able to capture the distinctive features from the ECG signals. Hence, the network can be trained from these learned features even without big data, achieving desirable diagnostic performance. On the other hand, the automated analysis of EMG and EEG signals is more challenging as these signals are more chaotic in nature. Therefore, it is more complicated for the network to learn from the hidden and subtle information present in these signals.

During the content review, we have studied the DL algorithm types used for their research works. Table 6 shows the number of studies that used a particular DL algorithm to analyze a specific physiological signals. CNN was used in 5, 15, 10 and 2 research works on EMG, EEG, and ECG respectively. Overall, CNN was used 32 times, that makes it by far the most popular DL algorithm. At the bottom of the table is LSTM which was only used for ECG processing.

Table 6: Summary of various DL algorithms applied to different physiological signals.

| DL algorithm | EMG | EEG | ECG | EOG | Total |
|-----------------------|-----|-----|-----|-----|-------|
| CNN | 5 | 15 | 10 | 2 | 32 |
| DNN | 2 | 1 | 2 | 0 | 5 |
| DBN | 0 | 3 | 0 | 2 | 5 |
| RBM | 0 | 2 | 2 | 0 | 4 |
| Autoencoder | 0 | 1 | 1 | 1 | 3 |
| RNN | 1 | 0 | 1 | 0 | 2 |
| Deep learning network | 0 | 2 | 0 | 0 | 2 |
| Robust deep learning | 0 | 0 | 1 | 0 | 1 |
| LSTM | 0 | 0 | 1 | 0 | 1 |

Apart from the algorithms, we have also studied the type of data used to conduct these studies. Table 7 indicates a summary of the data type used to implement the DL algorithm. Row one indicates that 28 studies were conducted using the public databases. Only 20 studies used private databases and 3 studies have used both databases. 16 out of 17 studies using ECG and 8 out of 23 studies on EEG have used public data. Indeed, 12 studies have used private EEG data to implement the deep learning algorithms.

Table 7: Summary of data type used to implement the DL algorithm.

| | EMG | EEG | ECG | EOG | Total |
|------------------------------|-----|-----|-----|-----|-------|
| Publicly available databases | 3 | 8 | 16 | 1 | 28 |
| Private databases | 4 | 12 | 1 | 3 | 20 |
| Both | 1 | 1 | 0 | 1 | 3 |
| Not reported | 0 | 2 | 0 | 0 | 2 |
| Number of papers | 8 | 23 | 17 | 5 | 53 |

Conventional machine learning approaches require lots of time and effort for feature selection. These features must extract relevant information from huge and diverse data in order to produce the best diagnostic performance. Furthermore, the best algorithm is unknown and thus, a lot of trial and error is necessary to select the best feature extraction algorithms and classification methods to develop a robust and reliable decision support systems for the physiological signals.

On the other hand, deep learning eliminates the need for feature extraction and feature selection. The decision-making algorithm can consider all available evidence [155].

The training algorithms for deep learning systems have a high computational complexity. Hence, this results in a high run-time complexity which translates into a long training time [156, 157, 158]. This will be a problem during the design phase, because during this phase a designer must decide what deep learning architecture to use. Once the architecture is chosen, the tuning parameters must be adjusted. Both the structure selection and parameter adjustment will basically influence the model. Hence, it is necessary to have many test runs. Shortening the training phase of deep learning models is an active area of research [159]. The challenge is speeding up the training process in a parallel distributed processing system [160]. The network between the individual processors becomes the bottle neck [161]. Graphics Processing Units (GPUs) can be used to reduce the network latency [162].

For this state of the art technology, the training time may be an issue, because it can influence the model selection strategies. To be specific, none of the reviewed papers approached the model selection process with statistical methods, such as cross validation [163]. We can only assume that the deep learning architectures, used in the reviewed scientific work, were selected based on single run trial. Similarly, we have to assume that the hyperparameters were also optimized by training the network once. This is a serious shortcoming, because these statistical validation methods reduce the sample selection bias [164, 165].

In addition, the use of deep learning can also be extended from one-dimensional physiological signals to two-dimensional medical images. Researchers are also exploring the benefits utilizing deep learning in medical image analyses [166]. It was reported that the automated staging and detection of Alzheimers disease, breast cancer, and lung cancer has shown optimistic diagnostic performances.

5. Conclusion

In this paper, we reviewed 53 papers on deep learning methods applied to healthcare applications based on physiological signals. The analysis was carried out in two distinct steps. The first step was bibliometric keyword analysis based on the co-occurrence map. This analysis step reveals the connection between the topics covered in the reviewed papers. We found four distinct clusters, one for each physiological signal. That result helped us to structure the second analysis step, which focuses on the paper content. As such, the paper content was established by extracting the specific application area, the deep learning algorithm, system performance, and the types of dataset used to develop the system.

The fact that deep learning algorithms performs well with large and diverse datasets which has two consequences. First, the dataset becomes critically important for the system design. Therefore, we focused our efforts on this criterion during our analysis. We found that, the scientific work, documented in 31 of the reviewed papers, was based on one or more freely available datasets. Therefore, we predict that the importance of these freely available public datasets may increase. The other consequence is that deep learning algorithms will perform well in practical settings, because clinical routine produces lots of data with large variations. However, none of the reviewed papers verified this in a practical setting. Another fundamental point is that, our literature survey yielded only 53 papers. The small number of studies imply that there is scope for future work. To be specific, 53 papers do not reflect the comprehensive healthcare applications based on the physiological signals. In future, there may be more advanced deep learning algorithms focused on the early detection of diseases using physiological signals.

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Acronyms

| | |
|-------------|----------------------------------|
| AED | Automated External Defibrillator |
| ANN | Artificial Neural Network |
| BCI | Brain Computer Interface |
| CNN | Convolutional Neural Network |
| CVD | Cardiovascular Disease |
| DB | Database |
| DBN | Deep Belief Network |
| DL | Deep Learning |
| DNN | Deep Neural Network |
| ECG | Electrocardiogram |
| EEG | Electroencephalogram |
| EMG | Electromyogram |
| EOG | Electrooculogram |
| GMM | Gaussian Mixture Model |
| GPU | Graphics Processing Unit |
| K-NN | K-Nearest Neighbour |
| LSTM | Long Short-Term Memory |
| OSA | Obstructive Sleep Apnea |
| RBM | Restricted Boltzmann Machine |
| RNN | Recurrent Neural Network |
| SVM | Support Vector Machine |

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Appendix A. Cluster description

Table A.8: Author supplied keywords mapped to topics

| Topic | Author supplied keywords |
|-------------|------------------------------------------------------------------------------------------------------------------------------------------------------------------------------------------------------------|
| arrhythmia | arrhythmia, arrhythmic signal identification |
| cvd | cardiovascular diseases, myocardial infarction, non-shockable, shockable, ventricular arrhythmias |
| db | mit-bih arrhythmia database, physiobank mit-bih arrhythmia database |
| dnn | deep neural network, deep neural networks |
| ecg | apnea- electrocardiogram signals, ecg, ecg measurement system, ecg signal, ecg signals, electrocardiogram, electrocardiogram signal quality classification, electrocardiogram signals, electrocardiography |
| heartbeat | heartbeat, heartbeat interval features, rr interval |
| measurement | computerised instrumentation, pollution measurement, power line interference |
| noise | denoising autoencoder, noise, noise measurement, snr |
| testing | testing |
| training | training, training data |
| wearable | wearable computers, wearable electrocardiogram measurement system, wearable fnirs |

| | |
|------------------|--------------------------------------------------------------------------------------------------------------------------------------------------------------------------------------------------------------------|
| algorithm | ada-boost, algorithm, algorithms, classification algorithms, component analysis, compression, hidden markov models, independent component analysis |
| dbn | belief networks, boltzmann machines, convolutional deep belief networks, dbn, deep belief network, rbm, restricted boltzman machine (rbm), restricted boltzmann machine, deep neural network, deep neural networks |
| eeg | brain signals, eeg, eeg data, eeg-based hand squeeze task, electroencephalography, electroencephalography (eeg), encephalogram signals |
| feature | feature clustering, feature extraction, feature learning, feature-extraction, features, unsupervised feature learning |
| learning machine | deep feature learning, deep learning, ensemble learning |
| model | machine, machines |
| motor imagery | mathematical model, model, models |
| sleep | motor imagery |
| classification | apnea detection, automatic sleep stage classification, obstructive sleep apnea detection, sleep apnea, sleep stage classification, slow eye-movements |
| control | classification, emotion classification, patient-specific eeg classification, pattern classification |
| emg | multifunction myoelectric control, myoelectric control |
| ml | electromyogram, electromyography, emg-based speech recognition, non-stationary emg, surface emg |
| prostheses | machine learning, machine learning algorithms |
| recognition | prostheses, prosthetics, upper-limb, upper-limb prostheses |
| signal | brain activity recognition, pattern recognition, pattern-recognition, recognition, signal recognition |
| bci | medical signal detection, medical signal processing, signal classification, signal reconstruction, signal representation, signals, time preserving signal representation strategy |
| cmn | bci brain computer interface, brain computer interface (bci), brain computer interfaces, brain-computer interface, brain-computer interface (bci), brain-computer interfaces |
| epilepsy | cnn, convolution, convolution neural network, convolutional neural network, convolutional neural networks, convolutional neural networks (cnns) |
| nn | epilepsy, seizure |
| real-time | batch normalization layers, biological neural networks, feedforward neural nets, neural-networks, neurons |
| system | real-time, real-time heart monitoring, real-time systems, truenorth-enabled real-time classification |
| | ibm truenorth neurosynaptic system, low-power platform, system |